Interactive Previewing for Transfer Function Specification in Volume Rendering

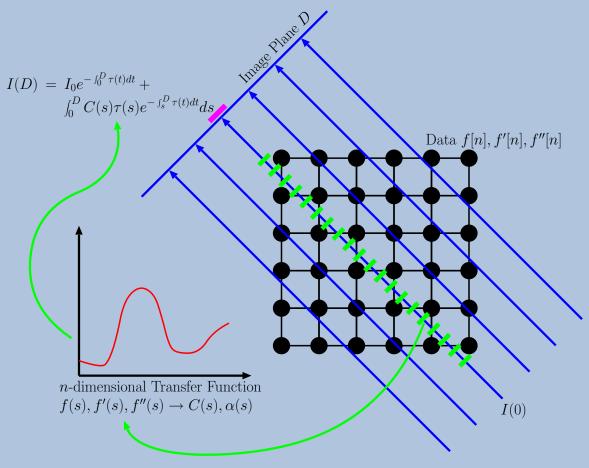
Charl P. Botha and Frits H. Post Data Visualisation Group, TU Delft The Netherlands

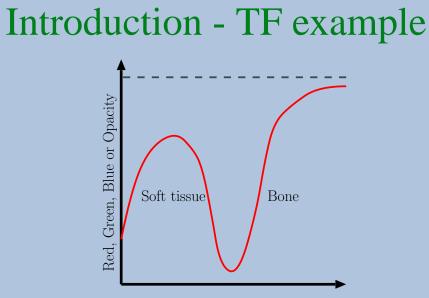
http://visualisation.tudelft.nl/

IEEE TCVG Symposium on Visualization 2002, Barcelona, Spain

∍First ●Prev ●Next ●Last ●Go Back ●Full Screen ●Close ●Qui

Introduction - DVR Refresher





Density of Voxel [Hounsfield Units]

Example Transfer Function for rendering CT-data

Introduction - Background

- DVR important visualisation technique
- Important component: Transfer Function
 - Data values \rightarrow Optical properties
- TF specification: prohibitively difficult
- New scheme
 - Feedback-based (DVR preview)
 - Current TF quality \leftrightarrow domain-specific comprehension/expectation
 - Simple; requires no special hardware

Introduction - Preview

Our work:

- slice-based DVR preview
- overlaid on greyscale slice of data
- serves as real-time feedback on DVR changes

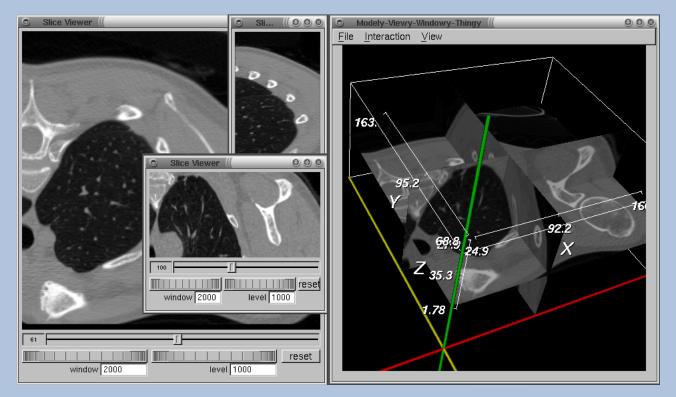


Related Work on TF Specification

- Trial-and-error with DVR feedback
- Design galleries
- Bajaj's Contour spectrum
- Kindlmann's semi-automatic TF generation
- Trial-and-error and design-galleries
 - feedback-based
 - real-time rendering, continually changing TFs
 - no explicit data-DVR relation

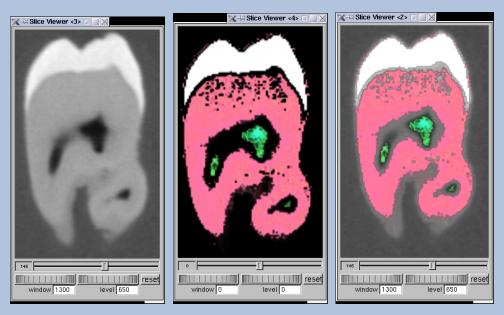
New method: fast, explicitly registered feedback; extension of our previous work.

Method - Clinical Expertise



Method - Overlaid feedback scheme

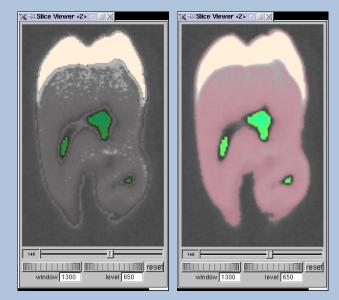
- Greyscale $X = \langle C_g, \alpha_g \rangle$
- Mapping $M = \langle C_m, \alpha_m \rangle = f(v)$
- Alpha-Blending $(1 \alpha_m)X + \alpha_m M$:



Method - Mappings

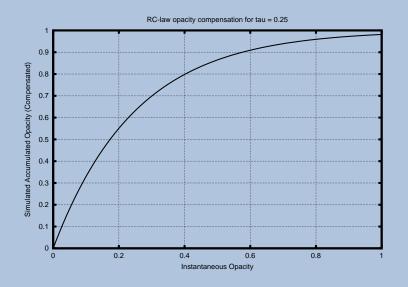
Mappings M = f(v):

 $\langle M = C_t * \alpha_t, \alpha_t \rangle$ vs $\langle M = C_t, c_{rc}(\alpha_t) \rangle$



Method - RC-law compensation

- DVR absorption $I(D) = I_0 e^{-\int_0^D \alpha(t) dt}$
- Simulate integral accumulation: RC-law opacity
- Instant \rightarrow Integral: $c_{rc}(\alpha_t) = 1 e^{\frac{-\alpha_t}{\tau}}$





Method - FD estimation of DVR

Need more accurate way to estimate accumulation:

$$I(D) = I_0 e^{-\int_0^D \tau(t)dt} + \int_0^D C(s)\tau(s)e^{-\int_s^D \tau(t)dt}ds$$

can be reduced to:

$$I(0) = I_D e^{-N\alpha_k} + C_k \alpha_k \frac{1 - e^{-N\alpha_k}}{1 - e^{-\alpha_k}}$$

without too much cheating*.

Method - FD estimation of DVR: *

$$I(0) = I_D e^{-N\alpha_k} + C_k \alpha_k \frac{1 - e^{-N\alpha_k}}{1 - e^{-\alpha_k}}$$

- 1. Ray is cast through N voxels with identical (or very similar) C_k and α_k .
- 2. Ray-sampling distance Δs is of the same dimension as a voxel.

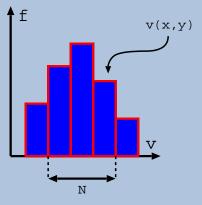
Method - FD estimation of DVR

Previewing single slice:

- 1. Iterate through each v(x, y) in current slice:
 - Transform to $\langle C_t, \alpha_t \rangle$.
 - Optional: perform shading.
 - \bullet Calculate N.
 - Evaluate simplified equation.
- 2. Blend with greyscale.

Answers question for all slice voxels: What would the result be of casting a ray through *all* the optical material represented by the current voxel.

Method - FD estimation of DVR For every v(x, y) in slice, we need N:

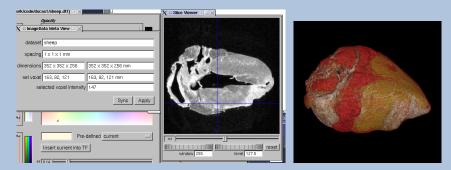


Frequency distribution for (x, y)

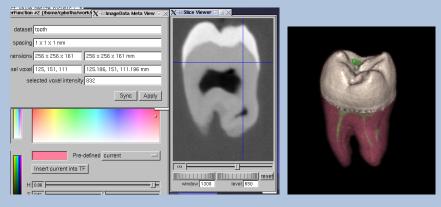
- 1. Get FD for current (x, y)
- 2. Binary search bin containing current v(x, y)
- 3. Perform merging based on C_t and α_t
- 4. N is number of voxels in merged bins.

Results

MRI data of a sheep heart:



CT data of a tooth:



... another tooth preview.

Conclusions

Interactive Previewing for TF specification

- Simple to implement
- Fast, requires no special hardware
- Feedback on visibility and optical characteristics
- Voxel-registration: correspondence, fidelity
- Small changes visibly, incrementally fed back
- Effective use of user's knowledge of the data
- Super-imposed segmentation = expectations
 ⇒ TF optimised
- Speeds up TF specification

Acknowledgements

This research is part of the DIPEX (Development of Improved endo-Prostheses for the upper EXtremities) program of the Delft Interfaculty Research Center on Medical Engineering (DIOC-9).